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(54) Title: AN AGGREGATE FOR TRANSLUMINAL INSERTION OF A TUBULAR STENT, AND AN ENDOVASCULAR GRAFT DEVICE <div data-bbox="386 1150 1279 1354" data-label="Image"> </div> (57) Abstract <p>An aggregate for transluminal insertion of a tubular stent (1) which, in its placed condition in a vessel in the vascular system, is provided at its periphery with a tubular coating (2) along at least part of its length, the aggregate including an introducer sheath (3) with a stent arranged inside the sheath in a first condition with a reduced diameter, and an extruder device (4) which can be manipulated to release the stent from the introducer sheath, the stent (1) being adapted to expand to a second condition with a larger diameter. The stent is placed in its first condition inside the introducer sheath (3) in direct contact with the inner sheath surface, and the tubular coating (2) is placed in connection with the aggregate so that the coating is not placed on the periphery of the stent until during the release of the stent from the introducer sheath by the expansion from the first to the second condition.</p>		

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An aggregate for transluminal insertion of a tubular stent, and an endovascular graft device

The present invention relates to an aggregate for transluminal insertion of a tubular stent which, in its placed condition in a vessel in the vascular system, is provided at its periphery with a tubular coating along at least part of its length, which aggregate includes an introducer sheath with a stent arranged inside the sheath in a first condition with a reduced diameter, and an extruder device which can be manipulated to release the stent from the introducer sheath, the stent being adapted to expand to a second condition with a larger diameter.

Such an aggregate is known from EP-A-0 539 237. This prior-art aggregate is intended for use in the repair of an abdominal aortic aneurysm, where a graft consisting of a stent and a blood-impermeable tubular coating arranged at the periphery of the stent is inserted in the aorta at the aneurysm and placed in such a manner that the graft cuts off the aneurysm from the bloodstream in the aorta. A number of other stents provided with a tubular coating are also known, vide, for example, WO95/05132, in which the stent is placed in or permanently connected with the tubular material, WO93/22986, in which a stent for placement in the oesophagus is provided with a tubular coating at the stent middle, but the stent ends are uncoated, and the publications EP-A-0 696 446 and WO94/24961, in which the stent is embedded in the tubular material.

The prior-art stents with a tubular coating suffer from the disadvantage that they are inserted by means of an introducer sheath of a relatively large external diameter, typically from 6.0 to 8.7 mm (18-26 French). This necessitates femoral insertion and surgical

incision at the site of insertion to provide space for passage of the introducer sheath into the vascular system.

The object of the present invention is to provide
5 an aggregate rendering possible true percutaneous insertion of a stent and a tubular coating by means of the Seldinger technique.

In view of this, the above aggregate is characterised in that in that the stent is arranged in
10 its first condition at least partially inside the introducer sheath in direct contact with the inner sheath surface, and that at least the major part of the tubular coating is positioned separate from the periphery of the stent while the stent is in its first
15 condition.

With this arrangement of the tubular coating in connection with the aggregate, the coating is not placed on the periphery of the stent until during the release of the stent from the introducer sheath by the expansion
20 from the first to the second condition.

By mounting the tubular coating in the aggregate in such a manner that it is not placed directly on the outer surface of the stent, the stent can be arranged in direct contact with the inner surface of the
25 introducer sheath. This means that the internal diameter of the introducer sheath can be made smaller than in prior art, partly because space is not required for both the body material of the stent and for the coating at the same place inside the sheath, partly because the
30 body material of the stent, typically a filamental metallic material, can more easily be packed into a compact configuration when the stent material is free of the tubular coating. With this design of the aggregate it is possible to arrange the stent inside an
35 introducer sheath having an external diameter of about

5.3 mm (16 French) or less, typically ranging from 2.7 to 5.3 mm (8-16 French).

The aggregate according to the invention renders possible insertion by other routes than the femoral one; 5 the percutaneous insertion may, for example, be effected axillarily (at the armpit), radially (through the arm), cervically (at the throat) or elsewhere having a vessel of medium or large size located close to the skin. The largest introducer sheath that can be used with the 10 Seldinger technique has an external diameter of 16 French. In addition to rendering possible other access routes than the femoral one, the invention also provides advantages in case of femoral percutaneous insertion. The puncture hole at the site of insertion is substan- 15 tially smaller than with the known techniques, which is partly less traumatic to the patient, partly produces less bleeding out of the puncture hole at replacement of introducer sheath, catheters, etc. The loading method of the stent into the introducer sheath is thus of 20 substantially less importance than in prior art, vide the mention of "muzzle loading" as opposed to "breach loading" in EP-A-0 539 237.

In one embodiment the tubular coating may at some positions be connected with the stent, preferably at the 25 place on the stent length being at or closest to the distal end of the introducer sheath. The connection between the stent and the coating provides the advantage that the coating is placed on the periphery of the stent in a predetermined position along the length of the 30 stent when the stent is placed at the desired site. The connection will typically have been made at one end of the coating, and it is normally sufficient that the stent is provided with a single-layer coating. However, it is possible to effect the connection at another 35 location on the coating, such as at the middle thereof,

the result of which is that at least along part of its coated length the stent becomes provided with a two-layer coating. The coating may be connected with the distal end of the stent or be connected with the stent at a distance therefrom proximally to this end. In this connection the distal end means the leading end during the insertion, and the proximal end means the following end inserted as the last one. If the coating is connected at a distance from the distal end of the stent, the stent portion distally from the connection must be kept in the first position by a member being separate from the introducer sheath so that the coating may pass radially in between the sheath and the member and thereby reach the fastening location. Preferably the coating is connected with the stent at points or along a circular path located in a plane at right angles to the longitudinal axis of the stent. The connection may, for example, be effected by means of suture, glue, engagement means embedded in the coating or by the coating being shaped around one or more pieces of material in the stent body.

In an alternative embodiment the aggregate keeps the tubular coating completely separated from the stent until the release of the latter has commenced. The coating is thus not fastened to the stent. This provides the advantage that no separate fastening means, such as suture or glue, have been used that may act as foreign bodies in the body after the placement and that may further take up space while the stent is inside the introducer sheath in its first condition.

In a preferred embodiment of the aggregate, the tubular coating surrounds the introducer sheath. After the placement, the coating has a diameter corresponding to the diameter of the stent in its second, expanded condition. Most frequently, the coating is not very

elastic or substantially inelastic, and this means that the coating has a circumferential length substantially larger than the circumferential length of the inner surface of the introducer sheath. By arranging the coating around the introducer sheath, the outer surface of which has a larger circumferential length than the inner surface, the coating need not be folded or bent as much together as at an arrangement inside the sheath. The external arrangement therefore facilitates the spreading of the coating at the expansion of the stent to a larger diameter. With the external location it is also possible to mount the coating in the aggregate so that in the longitudinal direction it is extended over a length which is not smaller than the coated length on the outer surface of the stent after the placement. Folding of the coating in the longitudinal direction is thus avoided, which contributes to the coating only causing a relatively small diameter increase for the total aggregate. A further advantage is that the stent is only put in touch with the inner surface of the coating when the stent begins expanding to a larger diameter after its extrusion through the distal end opening of the introducer sheath. Thus, the introducer sheath contributes to an orderly placing of the coating on the outer stent surface.

The aggregate may comprise a catheter surrounding the tubular coating and the introducer sheath until the aggregate has been transluminally advanced to a location close to the site of placement. The catheter protects the coating during the advancing from the puncture hole to the area near the site of placement where the introducer sheath is extruded through the distal opening of the catheter before placement of the stent is commenced. It is possible to advance the catheter in the vessel before the introducer sheath with the coating and

the stent is inserted into the patient, but normally the whole aggregate is preferably inserted at the same time because this renders it possible to advance the introducer sheath through the catheter in advance and
5 under orderly circumstances while the catheter assumes a straight shape. If the catheter is to be advanced in the vascular system along a route having considerable curves for positioning at a site of placement with a small vessel lumen, it may, however, be advantageous
10 first to insert the catheter together with a guidewire and then to retract the guidewire from the patient, whereupon the introducer sheath is pushed forward through the catheter. In this case the inner surface of the catheter may be formed in a manner reducing friction
15 between the sheath and the inner catheter surface. Such a separate advancing of the introducer sheath renders it possible to place a stent coating at a site of a very small vessel lumen and a correspondingly small diameter of the stent in its second, expanded condition.

20 In one embodiment the aggregate comprises an annular cavity in which the tubular coating lies protected until release of the stent. The annular cavity may be formed by the outer surface of the introducer sheath and the inner surface of a catheter, viz.,
25 corresponding to the embodiment just mentioned. Another possibility is to form the annular cavity with an outer wall which surrounds the tubular coating and has an external diameter substantially corresponding to the external diameter of the introducer sheath. Thus the
30 whole aggregate may have an external diameter which corresponds to the sheath and is smaller than the outer diameter of said catheter.

In a preferred embodiment the cavity is formed in the distal end of the introducer sheath, preferably by
35 the sheath at this end having an elongated recess

shielded inwards by means of a tube of a material which is flexible and substantially unstretchable. As the inner shielding tube is made of an unstretchable material it can absorb the radial pressure from the 5 stent loaded into the introducer sheath as hoop stresses in the tube material so that the radial pressure from the stent does not affect the tubular coating which has been received in the annular space between the shielding tube and inner surface of the introducer sheath. At the 10 same time the shielding tube may, by suitable choice of its material, be bending flexible so that the distal end of the aggregate is suitably soft to facilitate advancement through the vessels and avoid damage to the vessel walls. The recess and thus the annular space may have 15 a suitably large size in the radial direction so that the coating may be arranged in a bellows-shaped pattern in the recess, whereby the recess achieves shorter length. Preferably, however, the recess has a length corresponding to the length of the coating, and a radial 20 depth suitably small so that the coating can just be received in the recess, the aggregate thus obtaining an advantageously small external diameter.

If it is not desired to provide the stent with a coating in one or both end sections so as to obtain a 25 stronger fixation of the stent ends to the vessel in which the placement is effected, the stent is preferably arranged around the extruder device extending centrally through the introducer sheath, the stent in its first condition being located partially in the distal section 30 of the introducer sheath, partially in an annular cavity in the head of the extruder device, and the distal end of the tubular coating being arranged proximally at a distance from the distal end of the stent. When the stent is placed, the distal end section of the stent 35 lying radially compressed in the head of the extruder

device during the insertion may expand for fixation against the vessel wall without being provided with coating. At the proximal end of the stent, a coating-free end section can be established by the coating being
5 suitably shorter than the stent body in its second, radially expanding condition.

The stent may be formed so that it is self-expanding and largely does not change its length at the expansion. Stents of this type are applicable in
10 connection with the invention. Alternatively the stent may be formed so that its length is reduced at the expansion from the first to the second condition. This means that after engagement with the inner surface of the tubular coating an expanding stent area obtains a
15 shorter length at the continued expansion. Thus, the stent is prevented from affecting the coating with longitudinal tensile stresses. On the contrary, the stent may contract the coating somewhat, which cannot overload the material of the coating. At the same time
20 the coating is not able to lock the expanding stent material in an intermediate position without full expansion.

It may be an advantage when the tubular coating is arranged in a folded condition around the introducer
25 sheath that the surfaces facing the introducer sheath are at least partially in contact with an adhesive. The adhesive retains the coating on the outer surface of the introducer sheath until the stent begins to spread out the coating at the start of the expansion, which breaks
30 the bond produced by the adhesive between the coating and the sheath. Preferably, the adhesive is arranged as far as possible on the outer sheath surface so that after placement of the stent the sheath has no substantial amount of adhesive left.

The present invention further relates to an endovascular graft device comprising at least a first stent for fixation against a vessel wall in the vascular system and a second stent for placement fully or
5 partially inside the first stent as well as a tubular coating. Such a graft device is known from EP-A-0 551 179 for repair of an abdominal aortic aneurysm. The first stent is here placed on the infrarenal aorta portion upstream of the aneurysm, whereupon the cranial
10 ends of two graft devices with permanent coatings on the stents are balloon expanded for fixation with their cranial end openings located on a level with the cranial end opening in the first stent. The first stent serves to protect the aorta wall against the relatively large,
15 radially outward pressure influences occurring when the two grafts are balloon expanded. Of necessity, these forces have to be large to deform the caudal ends of the two grafts to cover the circular cross-section in the first stent.

20 The object of the graft device according to the invention is to anchor a stent with a tubular coating at a site where the vessel wall does not have sufficient extent to provide a safe mounting of a coated stent graft. In view of this the graft device is characterised
25 in that before the placement at the first stent the second stent and the tubular coating are mounted in an aggregate according to any one of claims 1 to 10, that the first and the second stents have substantially the same diameter in said second condition with a larger
30 diameter, and that after placement the tubular coating is at least partially fixed between the inner surface of the first stent and the outer surface of the second stent. In addition to achieving said insertion advantages of the aggregate, the coating is fixed very
35 securely by the squeezing between the two stent bodies.

This is an advantage, for example, if the coating hangs down past the caudal end of the second stent, which may be the case when the coating forms a trouser-shaped graft body with two lower openings each provided with
5 a separate graft body, as described by the Applicant in WO95/16406.

Another advantage of the graft device is that the first stent may be formed as a relatively open stent of a heavy material and may be placed so that it extends
10 from the top and some way down past the renal arteries, whereupon the second stent may be placed inside the first one in a position where the coating is arranged infrarenally. This permits the bloodstream to the renal arteries to pass the graft device without being hindered
15 by the coating, and at the same time the second stent is supported by the caudal end section of the first stent, which is securely fixed to the aorta wall suprarenally. Such a graft device is especially suitable for repair of abdominal aortic aneurysms in which the
20 infrarenal aorta portion upstream of the aneurysm is very short.

Examples of embodiments of the invention will now be described in further detail below with reference to the drawing, in which

25 Figs. 1-6 show longitudinal sections through the distal ends of six different embodiments of the aggregate according to the invention,

Figs. 7 and 8 are two different stages in the placement of the stent from the embodiment shown in Fig.
30 6,

Figs. 9-12 show four different stages of the insertion and release of the stent in a seventh embodiment of the aggregate,

Figs. 13 and 14 are cross-sectional views of
35 transverse folds in a tubular coating,

Fig. 15 is an illustration of a graft device according to the invention positioned at an abdominal aortic aneurysm, and

Fig. 16 is a cross-sectional view through an
5 introducer sheath with an annular cavity in which a coating is positioned.

In the subsequent description of the different embodiments the same designations of the main elements of the invention are used for the sake of simplicity.
10 The main elements of the aggregate are a tubular stent 1, a tubular coating 2, an introducer sheath 3 and an extruder device 4. In some embodiments the aggregate may also comprise a catheter 5.

The stent 1 may have many different designs. It
15 may, for example, be constructed from sets of wires which extend in a spiral shape with opposite directions of windings through the stent body, as described in German patent No. 33 42 798, or as described in US-A-5 370 683 be formed by a single wire bent in suitable
20 courses and laid in a spiral course, or as described in EP-A-0 645 125 be made of a wire bent and arranged in a course forming rhomboid cells, or be of the so-called Gianturco Z-stent type, or be formed as described in DE-A-39 18 736 or in WO94/03127. The stent may further be
25 formed by several wires bent together to form heart-shaped or arrow-shaped cells where the wires are wound about each other at the points of intersection or are knotted to form knots as partially described in the Applicant's WO 97/09945 (corresponding to Danish patent
30 application No. 995/95, which was made available to the public on 8 February 1996). With reference to the latter application the description therein of various stent designs is hereby incorporated into the present application.

The stent 1 is expandable from a first condition with a reduced diameter to a second condition with a larger diameter. For the fields of application mentioned in the following for the stent, ranges are mentioned for the typical stent diameter when assuming its second condition: coronary 2-4 mm; iliac, femoral and renal 6-12 mm; carotid 6-12 mm; aortic aneurysm 15-30 mm; vena cava 12-30 mm; vena subclavia 12-30 mm; arteriovenous shunt endoprosthesis 6-14 mm; TIPS (bypass in liver) 10-12 mm; ureter 4-7 mm; urethra 4-7 mm; oesophagus 18 mm at the middle; biliary 6-10 mm; pancreas 2-3 mm; and bronchial 15-20 mm. The stent material may be stainless steel, nitinol, titanium, tantalum, a copper alloy or a plastic material such as modified butadiene.

The tubular coating 2 may be of polyester (such as Dacron TM), polytetrafluoroethylene PTFE, polyurethane PU, polyethylene PE, propylene PP, nylon, carbon fibres or any other biocompatible material capable of blocking a bloodstream or another flow of body fluid. The coating may be of a foil which is completely impermeable, but the coating is preferably porous to promote fibrous ingrowth and thus anchoring of the coating in the body vessel in question. The porosity may be produced by arranging salt grains of a predetermined sieve dimension in the synthetic material and wash out the salt grains after establishment of the foil shape. The coating may also be made by weaving threads into a tubular body. Another possibility is to manufacture the foil from a porous expanded PTFE.

Fig. 1 shows the stent 1 arranged in its first condition with a reduced diameter inside the introducer sheath 3. The stent is received in a recess in the extruder device 4 which at the distal end has a head 6 lying protectively in front of the distal opening of the sheath. The rounded front end of the head facilitates

the advancement to the desired place or the pushing into a catheter, if such is used. If desired, the head 6 may be provided with a distally projecting soft guidewire portion. The annular proximal end wall 7 in the recess 5 pushes at the proximal end of the stent when the device 4 is moved forwards in relation to the sheath 3 or the sheath is pulled back. In addition, at axially separated places in the recess the device 4 may have projecting engagement members supporting the stent during the 10 placement. The foil or coating 2 is connected to the distal end of the stent and extends from the place of connection radially out between the distal end of the sheath and the backward end surface of the head 6. On the outer surface of the sheath the foil has been turned 15 back to a longitudinally elongated position in contact with the sheath.

The second embodiment shown in Fig. 2 deviates from the first one in that the head 6 has a sufficiently small diameter to pass through the inner lumen of the 20 sheath, and that the foil 2 is completely separated from the stent 1. This provides an extra possibility of variation at the insertion, viz., that the introducer sheath with the foil 2 is first inserted to the desired site, whereupon the device 4 with the stent is pushed 25 forward and placed. The distal end of the foil projects down about the distal opening of the sheath so that the rim of the foil is gripped by the outer surface of the stent at the beginning expansion of the stent when it is extruded through the distal opening.

30 The third embodiment in Fig. 3 shows a stent 1 with heart or arrow-tip-like lattice cells inserted in the sheath 3. Such a stent can be compressed to a very small diameter in the first condition as seen in relation to the diameter in the second condition. The foil 2 is 35 connected with the stent end, and at the annular rim of

the sheath 3 the head 6 has an annular recess 7 lying protectively around the foil end during the insertion.

The fourth embodiment shown in Fig. 4 is of a type in which the foil 2 is received inside an annular cavity 8 produced by the sheath 3 having at its distal end section an elongated recess which is inwardly shielded by means of a tube 9 of a material being flexible and substantially unstretchable. The tube 9 may, for example, be made of PTFE, of carbon fibre, of dacron or of mylar. Viewed in a longitudinal section, the foil 2 is arranged in a bellows-shaped pattern and the foil is pulled out of the distal annular opening of the recess when the stent is extruded. Fig. 5 shows a similar design in which the cavity 8 is so long that the foil can lie full-length in its longitudinal direction. The foil may, for example, be pre-mounted on the outer surface of the tube 9 before the latter is mounted in the sheath 3.

Fig. 6 shows a sixth embodiment in which the stent is arranged around the extruder device 4, which extends centrally through the introducer sheath 3. The stent is located partially in the distal section of the introducer sheath, partially in an annular cavity 10 in the head 6 of the extruder device. The distal end of the tubular coating 2 is located proximally at a distance from the distal end of the stent, and the coating is arranged on the outer surface of the sheath completely separated from the stent 1. The distal end of the coating lies inserted under a circumferential spring flap 11 on the outside of the head so that the coating retains its longitudinal location during the insertion to the desired site of placement.

Fig. 7 shows the beginning release of the stent at the site of placement. The release is effected by the sheath being moved backwards in relation to the head 6.

The released area of the stent 1 expands to a larger diameter and thus catches the coating 2. Then the head 6 can be moved away from the stent by the device 4 being pushed forwards so that the distal end of the stent 5 expands to its full diameter into engagement with the vessel wall 12 (see Fig. 8), whereupon the sheath 3 can be retracted from the patient. It can be seen that the foil 2 does not cover the distal end section of the stent. Alternatively, it is possible to fasten the foil 10 to the outer surface of the stent, the foil then in the mounted position in the aggregate passing into the space between the back of the head 6 and the front of the sheath 3.

Fig. 9 shows the stent 1 inside the sheath 3 and 15 the foil 2 on the outer surface thereof. The sheath is arranged in a catheter 5, and the subsequent Figures 10 to 12 show the extrusion of the stent 1 from the sheath with simultaneous fastening of the foil to the outer stent surface. The stent is extruded from the sheath 3 20 by means of an extruder device 4 in the form of a pusher.

Fig. 13 shows how the foil 2 can be folded on the outer surface of the sheath 3. Fig. 14 shows that the foil can be temporarily fastened to the outer sheath 25 surface by means of an adhesive 15. The folding allows for a rather great length of foil or covering to be received in little space.

Fig. 16 shows that the foil 2 can be received between the sheath 3 and the tube 9 folded in a wave- 30 shaped pattern in the circumferential direction. This embodiment is particularly advantageous when the foil 2 is positioned in a straightened longitudinal position, as shown in Fig. 5.

In Fig. 15, a first stent 20 is seen to be placed 35 at the renal arteries, and the stent 1 is here a second

stent provided with the coating foil 2, which cuts off an aneurysm from the aorta. The first stent 20 can be relatively open at least in the areas opposite the renal arteries so that the renal blood flows are unhindered.

5 The second stent is placed infrarenally inside the first one and the coating foil 2 is thereby fixedly locked in between the two stents in the area of their overlap.

The various embodiments described above can be combined to new embodiments within the present invention. Further, in the present context coating or foil includes any kind of covering or graft material to be positioned on the stent.

P A T E N T C L A I M S

1. An aggregate for transluminal insertion of a tubular stent which, in its placed condition in a vessel in the vascular system, is provided at its periphery with a tubular coating along at least part of its length, which aggregate includes an introducer sheath (3) with a stent (1) arranged inside the sheath in a first condition with a reduced diameter, and an extruder device (4) which can be manipulated to release the stent from the introducer sheath, the stent being adapted to expand to a second condition with a larger diameter, characterized in that the stent (1) is arranged in its first condition at least partially inside the introducer sheath (3) in direct contact with the inner sheath surface, and that at least the major part of the tubular coating (2) is positioned separate from the periphery of the stent while the stent is in its first condition.

2. An aggregate according to claim 1, characterized in that the tubular coating (2) is connected with the stent (1), preferably at the place on the stent length being at or closest to the distal end of the introducer sheath (3).

3. An aggregate according to claim 1, characterized in that the aggregate keeps the tubular coating (2) completely separated from the stent (1) until the release of the latter has commenced.

4. An aggregate according to any one of claims 1-3, characterized in that the tubular coating (2) surrounds the introducer sheath (3).

5. An aggregate according to claim 4, characterized in that the aggregate comprises a catheter (5) surrounding the tubular coating (2) and the introducer sheath (3), preferably until the aggregate

has been transluminally advanced to a location close to the site of placement.

6. An aggregate according to any one of claims 1-5, characterized in that the aggregate
5 comprises an annular cavity (8, 10) in which the tubular coating (2) lies protected until release of the stent.

7. An aggregate according to claim 6, characterized in that the cavity (8) is formed in the distal end of the introducer sheath (3), preferably
10 by the sheath at this end having an elongated recess shielded inwards by means of a tube (9) of a material which is flexible and substantially unstretchable.

8. An aggregate according to any one of claims 1-7, characterized in that the stent (1) is
15 arranged around the extruder device (4) extending centrally through the introducer sheath (3), that the stent in its first condition is located partially in the distal section of the introducer sheath, partially in an annular cavity (10) in the head of the extruder
20 device, and that the distal end of the tubular coating is arranged proximally at a distance from the distal end of the stent (1).

9. An aggregate according to any one of the preceding claims, characterized in that
25 the length of the stent (1) is reduced at the expansion from the first to the second condition.

10. An aggregate according to any one of claims 1-6, 8, 9, characterized in that the tubular coating (2) is arranged in a folded condition around the
30 introducer sheath (3), and that the surfaces facing the introducer sheath are at least partially in contact with an adhesive (15).

11. An endovascular graft device comprising at least a first stent for fixation against a vessel wall
35 in the vascular system and a second stent for placement

fully or partially inside the first stent as well as a tubular coating, characterized in that before the placement at the first stent (20) the second stent (1) and the tubular coating (2) are mounted in an aggregate according to any one of claims 1 to 10, that the first and the second stents (1, 20) have substantially the same diameter in said second condition with a larger diameter, and that after placement the tubular coating (2) is at least partially fixed between the inner surface of the first stent and the outer surface of the second stent.

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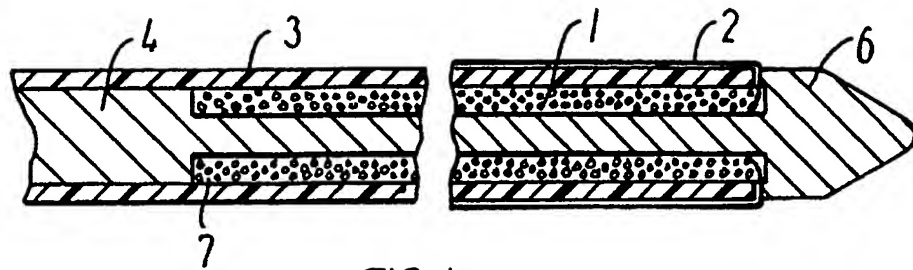


FIG. 1

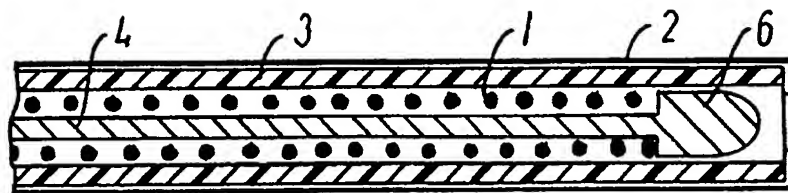


FIG. 2

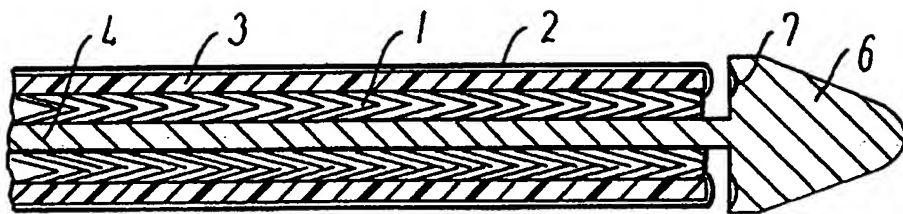


FIG. 3

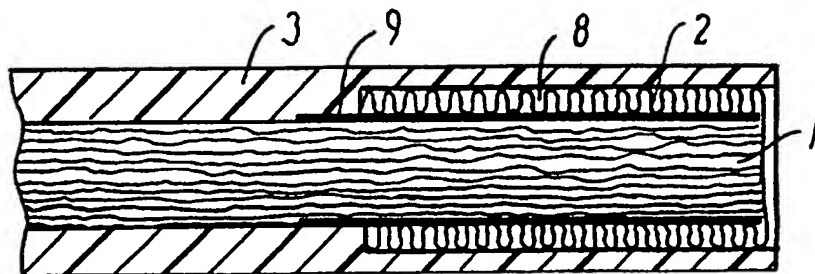


FIG. 4

2 / 4

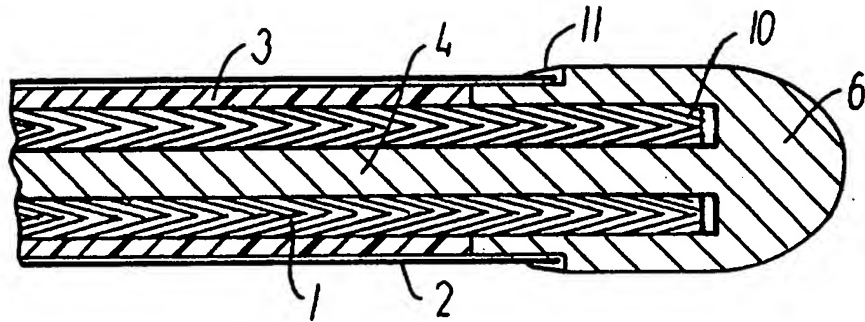


FIG. 6

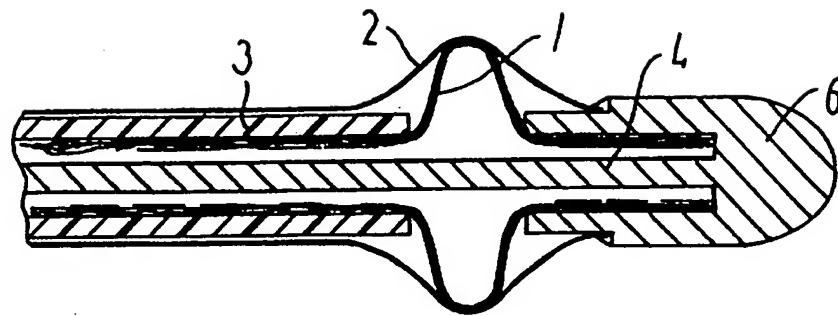


FIG. 7

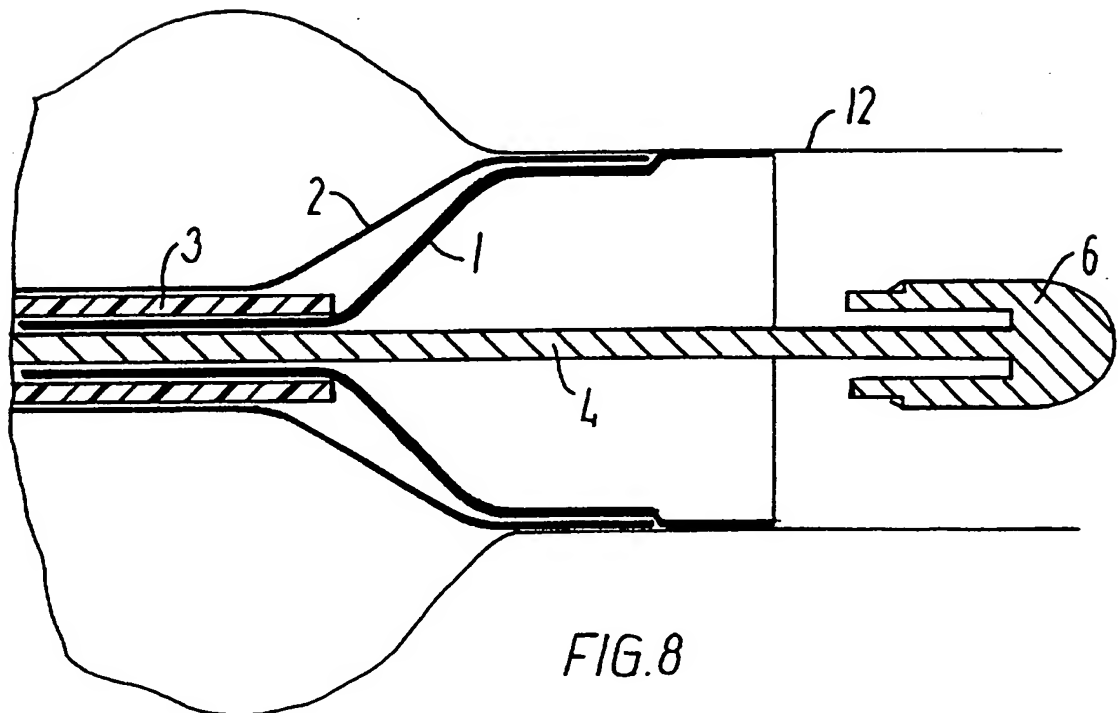


FIG. 8

3 / 4

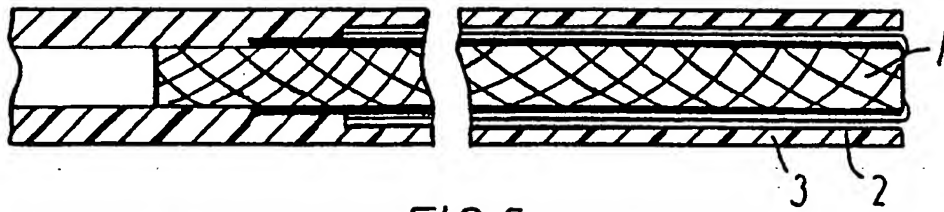


FIG. 5

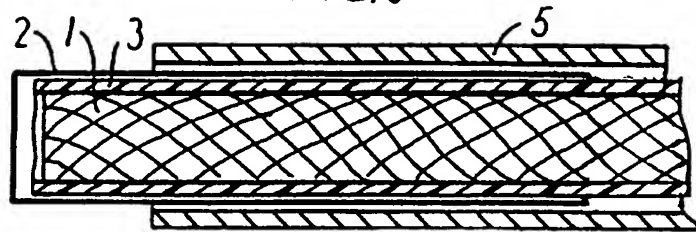


FIG. 9

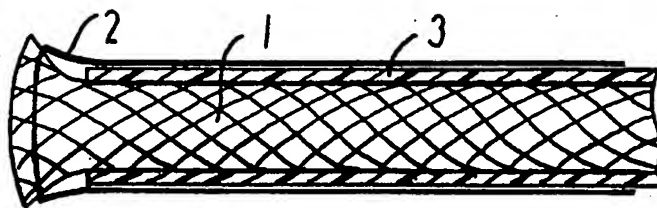


FIG. 10

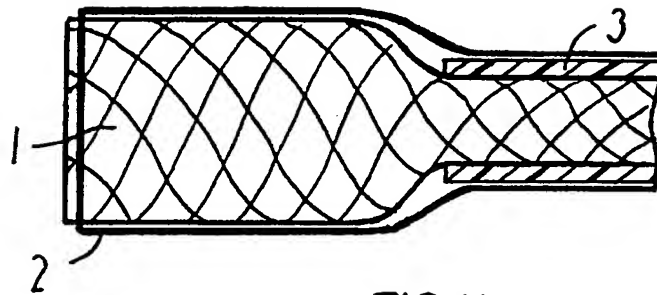


FIG. 11

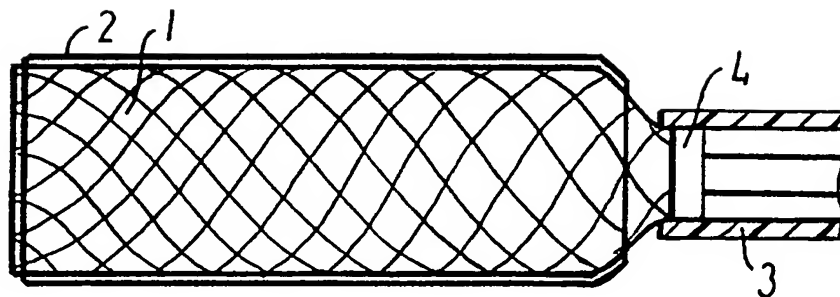


FIG. 12

4 / 4

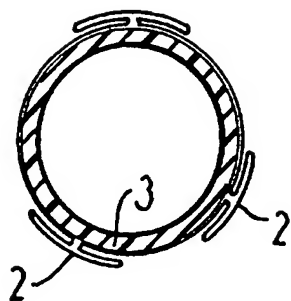


FIG. 13

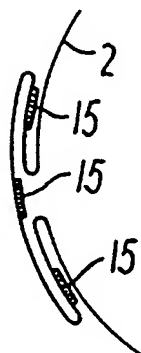


FIG. 14

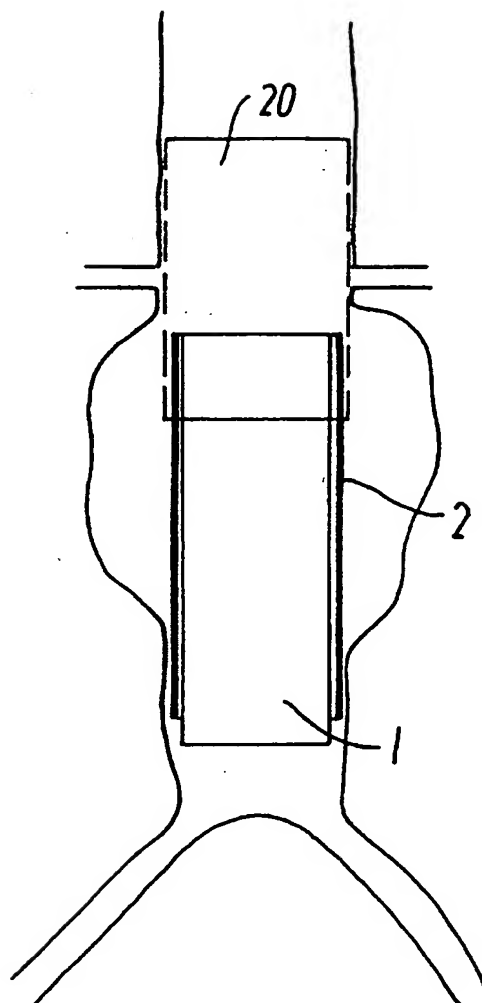


FIG. 15

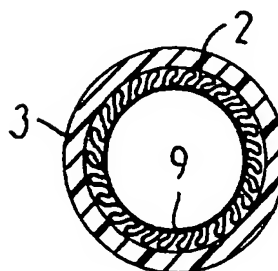


FIG. 16



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 6 : A61F 2/06	A3	(11) International Publication Number: WO 98/09583 (43) International Publication Date: 12 March 1998 (12.03.98)
(21) International Application Number: PCT/DK97/00370 (22) International Filing Date: 5 September 1997 (05.09.97) (30) Priority Data: 0961/96 6 September 1996 (06.09.96) DK (71) Applicant (for all designated States except US): WILLIAM COOK EUROPE A/S [DK/DK]; Sandet 6, DK-4632 Bjæverskov (DK). (72) Inventors; and (75) Inventors/Applicants (for US only): KAVTELADZE, Zaza A. [RU/RU]; ul. Mosfilmovskaya, 11-2-33, Moscow, 117330 (RU). KORSHOK, Alexandr P. [RU/RU]; ul. Potechina, 15-30, Ljuberezkij raion, Tromilino, Moskovskaya obl., Moscow, 130070 (RU). (74) Agents: INDAHL, Peter et al.; International Patent-Bureau, Høje Taastrup Boulevard 23, DK-2630 Taastrup (DK).		(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, GH, HU, ID, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZW, ARIPO patent (GH, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG). Published <i>With international search report.</i> <i>Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i> (88) Date of publication of the international search report: 16 April 1998 (16.04.98)
(54) Title: AN AGGREGATE FOR TRANSLUMINAL INSERTION OF A TUBULAR STENT, AND AN ENDOVASCULAR GRAFT DEVICE <div data-bbox="370 1163 1252 1371" data-label="Image"> </div> (57) Abstract <p>An aggregate for transluminal insertion of a tubular stent (1) which, in its placed condition in a vessel in the vascular system, is provided at its periphery with a tubular coating (2) along at least part of its length, the aggregate including an introducer sheath (3) with a stent arranged inside the sheath in a first condition with a reduced diameter, and an extruder device (4) which can be manipulated to release the stent from the introducer sheath, the stent (1) being adapted to expand to a second condition with a larger diameter. The stent is placed in its first condition inside the introducer sheath (3) in direct contact with the inner sheath surface, and the tubular coating (2) is placed in connection with the aggregate so that the coating is not placed on the periphery of the stent until during the release of the stent from the introducer sheath by the expansion from the first to the second condition.</p>		

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INTERNATIONAL SEARCH REPORT

International application No.

PCT/DK 97/00370

A. CLASSIFICATION OF SUBJECT MATTER

IPC6: A61F 2/06

According to International Patent Classification (IPC) or to both national classification and IPC

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C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 0539237 A1 (COOK INCORPORATED), 28 April 1993 (28.04.93), abstract --	1-11
A	US 5366473 A (THOMAS R. WINSTON ET AL.), 22 November 1994 (22.11.94), abstract -- -----	1-11

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Date of the actual completion of the international search

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Information on patent family members

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International application No.

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